# Recent development of hydrogen sulfidereleasing biomaterials as novel therapies: a narrative review

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### Key Words:

biomaterials; cardiovascular disease; H<sub>2</sub>S donors; hydrogen sulfide; wound healing

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## ABSTRACT

 $Hydrogen sulfide (H_S)$  has been reported as an endogenous gasotransmitter that contributes to the modulation of a myriad of biological signalling pathways, which includes maintaining homeostasis in living organisms at physiological concentrations, controlling protein sulfhydration and persulfidation for signalling processes, mediating neurodegeneration, and regulating inflammation and innate immunity, etc. As a result, researchers are actively exploring effective approaches to evaluate the properties and the distribution of H<sub>s</sub>S in vivo. Furthermore, the regulation of the physiological conditions of  $H_s$  in vivo introduces the opportunity to further study the molecular mechanisms by which H,S regulates cellular functions. In recent years, many H.S-releasing compounds and biomaterials that can deliver H.S to various body systems have been developed to provide sustained and stable H,S delivery. Additionally, various designs of these H,S-releasing biomaterials have been proposed to aid in the normal conduction of physiological processes, such as cardioprotection and wound healing, by modulating different signalling pathways and cell functionalities. Using biomaterials as a platform to control the delivery of H<sub>2</sub>S introduces the opportunity to fine tune the physiological concentration of H<sub>s</sub>S in vivo, a key to many therapeutic applications. In this review, we highlight recent research works concerning the development and application of  $H_{2}$ S-releasing biomaterials with a special emphasis to different release triggering conditions in in vivo studies. We believe that the further exploration of the molecular mechanisms underlying H<sub>s</sub>S donors and their function when incorporated with various biomaterials will potentially help us understand the pathophysiological mechanisms of *different diseases and assist the development of H*,*S-based therapies.* 

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# Introduction

Hydrogen sulfide  $(H_2S)$ , which had been previously regarded as a lethal toxic pollutant for centuries, is currently being explored as an endogenous gasotransmitter with the capability to not only contribute in the modulation of a myriad of biological signalling pathways but also to maintain homeostasis in living organisms at physiological concentrations.<sup>1-5</sup> Over the past decades, many experiments have been performed to investigate the respective role of  $H_2S$  in both physiological and pathophysiological activities in mammals.<sup>6-9</sup> Specifically, this small molecule diffuses freely through the cell membrane to initiate a variety of responses independent of transporters, membrane receptors or second messenger systems, and regulate many cellular functions through a series of intracellular signalling processes.<sup>10</sup>

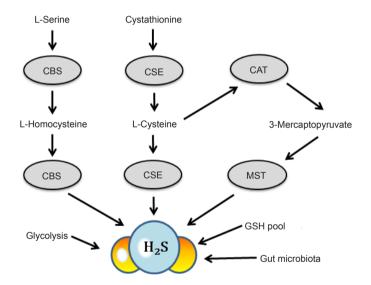
There is sufficient evidence to indicate the correlation between low concentration of endogenous  $H_2S$  and many pathophysiological diseases; namely, obesity, marked endothelial dysfunction, insulin resistance, high blood pressure, diabetes, exacerbated cardiac injury after ischemia/reperfusion injury, Alzheimer's disease, asthma, wound healing, and cancers.<sup>11-20</sup> Whether or not the  $H_2S$ -generating enzymes are

directly impaired in their respective molecular mechanisms does not differentiate between the presence or progression of these disease processes; therefore, the ability to re-establish the physiological concentration of aqueous  $H_2S$  *in vivo* will facilitate further exploration into the molecular mechanism of  $H_2S$  and how it regulates cellular functions.

Although there are a variety of H<sub>2</sub>S donors reported in studies mentioned above, including conventional inorganic donors like NaHS and Na<sub>2</sub>S and newly developed H<sub>2</sub>S donor with specific triggers, these donors are often with several issues such as instantaneous release profiles, low water solubility, and lacking capacity of in situ delivery.<sup>21, 22</sup> One promising strategy to address these issues is to incorporate these donors into biomaterials, either by physical entrapment or through covalent conjugation to polymers or macromolecules. In this review, by using the PubMed and Google-Scholar as the search engines, H<sub>2</sub>S, biomaterials and clinical terms of diseases as key words, we choose those literatures published after 2010 and focus on the recent development of novel biomaterials incorporating with the H<sub>2</sub>S-donor motifs for the controlled release of H<sub>2</sub>S in vivo. In particular, the synthesis and potential clinical applications of such materials are highlighted. More detailed introductions of the physiological roles and functions of  $H_2S$  can be found in some other excellent review articles published recently.<sup>7, 9, 23-26</sup>

### Homeostasis of Hydrogen Sulfide in Mammals

H<sub>2</sub>S is a colorless, flammable, water-soluble gas with strong rotten egg smell. In aqueous solutions, H<sub>2</sub>S is a volatile, weak acid that dissociates to form H<sup>+</sup>, HS<sup>-</sup> and  $\tilde{S}^{2-}$  (H<sub>2</sub>S  $\leftrightarrow$  H<sup>+</sup> + HS<sup>-</sup>  $\leftrightarrow$  2H<sup>+</sup> + S<sup>2-</sup>).<sup>27</sup> In mammals, H<sub>2</sub>S is produced endogenously from cysteine, serine, homocysteine and other substrates primarily through the actions of three major enzymes (Figure 1). Cystathionine- $\beta$ -synthase is mainly localized in the nervous system, brain and liver; cystathionine- $\gamma$ -lyase (CSE) is mainly localized in the cardiovascular system to produce H<sub>2</sub>S; and 3-mercaptopyruvate sulfurtransferase (3-MST) is predominantly localized in mitochondria.5, 20 In addition, the activities of gut microbiota, glycolysis and phosphogluconate of glucose, the glutathione and "sulfane sulfur" pools may also contribute to the maintenance of H<sub>2</sub>S concentrations in plasma and tissue (Figure 1),<sup>11, 28-30</sup> where sulfane sulfur is descriptive of the extremely reactive sulfur atom that is bonded to a divalent sulfur molecule, and thiocysteine and glutathione persulfide are two examples of biologically important compounds that contain a sulfate sulfur within their chemical makeup.<sup>11</sup>



**Figure 1.** Biosynthesis and catabolism of  $H_2S$ . In mammals,  $H_2S$  is produced endogenously from cysteine, serine, homocysteine, and other substrates primarily through the actions of three major enzymes. CBS is mainly localized in the nervous system, brain and liver; CSE is mainly localized in the cardiovascular system to produce  $H_2S$ ; MST is predominantly localized in mitochondria. In addition, the activities of gut microbiota, glycolysis and phosphogluconate of glucose, the GSH and "sulfane sulfur" pools may also contribute to the maintenance of  $H_2S$  concentrations in plasma and tissue.<sup>11, 28-30</sup> CAT: cystine aminotransferase; CBS: cystathionine- $\beta$ -synthase; CSE: cystathionine- $\gamma$ -lyase; GSH; glutathione;  $H_2S$ : hydrogen sulfide; MST: mercaptopyruvate sulfurtransferase.

Kenneth R. Olson<sup>31</sup> has reviewed different methods to detect the concentrations of  $H_2S$  within different samples of plasma/ blood. The distribution of  $H_2S$  varies in different tissues, fresh blood or plasma within animals. In blood, the concentration of  $H_2S$  has been reported to be ranging from 30–100  $\mu$ M.<sup>32-34</sup> The  $H_2S$  concentrations within brain tissue, the aorta and other homogenized samples from specific regions, in which  $H_2S$  may play significant roles, are higher than that within the blood, indicating that  $H_2S$  is an autocrine and paracrine messenger.<sup>35-37</sup>

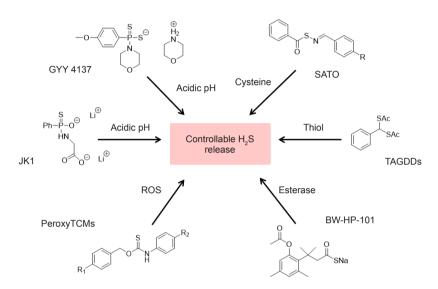
Due to its volatile nature, the stabilization of  $H_2S$  concentrations within *in vitro* experimentation is difficult because the equilibrium will shift to the left in the absence of glutathione, "sulfane sulfur"

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pools and gut microbiota. Several reports have been published showing that in cell culture wells, the  $H_2S$  concentrations will be halved in five minutes; this escape will be even faster when there is a bubbled tissue bath.<sup>38-41</sup> Coupled with the lipophilic characteristics of  $H_2S$ , direct intraperitoneal injections or blood administrations as described in previous reports will result in the rapid diffusion of  $H_2S$  out of the blood and into the lungs.<sup>42</sup> These bottlenecks have driven researchers to further explore the properties and delivery of  $H_2S$  with novel approaches, including the inventions of new  $H_2S$  donors and complexes of biomaterials capable of sustained and stable *in vitro* or *in situ* delivery of  $H_2S$ .

# Chemistry of Hydrogen Sulfide Donors and Release Mechanisms

For the controlled release of  $H_2S$ , many donors have been developed in the last decade. The conventional inorganic donors, including Na<sub>2</sub>S or NaHS, limit the prospects for mechanistic studies and medical applications due to their fast and uncontrolled  $H_2S$  release. To overcome this drawback, researchers have developed multiple types of  $H_2S$  donors with distinct properties, such as pH-sensitive donors,<sup>43-45</sup> enzyme-activated donors,<sup>46-48</sup> reactive-oxygen species,<sup>49</sup> and thiol-triggered donors<sup>50, 51</sup> (**Figure 2**).



**Figure 2.** Donor compounds for  $H_2S$  release. Recent advances in the development of  $H_2S$  donors has revealed multiple types of donors, namely, pH-sensitive donors including JK1 and GYY 4137,<sup>43-45</sup> enzyme-activated donors such as BW-HP-101,<sup>46-48</sup> reactive-oxygen species such as PeroxyTCMs,<sup>49</sup> and thiol-triggered donors including TAGDDs and SATO.<sup>50,51</sup>  $H_2S$ : hydrogen sulfide; TAGDD: thiol-activated gem-dithiol-based  $H_2S$  donor; SATO: S-aroylthiooxime; PeroxyTCM: PeroxyThioCarbaMate.

Among them, the pH-sensitive H<sub>2</sub>S donors have provided a new realm of scientific advances in specific pathophysiological diseases and processes that take place under specific acidic conditions such as acute cutaneous wounds.<sup>52</sup> Upon acute injury to cutaneous tissue, the acidic pH observed at the injury site decreases bacterial growth to help prevent infection; the progression of wound healing yields a gradual return to the physiological pH of 7.4.53 The longevity of H<sub>2</sub>S release under physiological conditions and its acceleration under acidic conditions is an important relationship to consider when developing H<sub>2</sub>S donors. Several pH-sensitive H<sub>2</sub>S donors have been evaluated for their respective efficacies; moreover, GYY4137 and JK1 are two commonly used pHsensitive H<sub>2</sub>S donors.<sup>43, 44, 50</sup> JKs are a group of pH-sensitive H<sub>2</sub>S-releasing compounds created under the manipulation of an intramolecular cyclization reaction and have shown to be efficient at monitoring H<sub>2</sub>S release<sup>45</sup>. Including H<sub>2</sub>S donors like GYY4137 and JKs can not only aid in the re-epithelialization of cutaneous tissue after trauma but also assists in decreasing inflammation and oxidative stress at the site of injury.54-58

Another highly beneficial development in the field of  $H_2S$  donors is the creation of enzymatically triggered donors such as BW-HP-101.<sup>46, 50, 59</sup> It can be averse to use triggers that

consume thiols or other cellular molecules that risk disrupting the chemical and redox balance of the environment; however, enzymatic triggers allow specific environments to be targeted without consuming these reactants. Additionally, enzymetriggered donors are advantageous as they rely on the presence of enzymes that are readily available within organisms. BW-HP-101 functions through a cascade initially mediated by an esterase, which is predominantly expressed in liver tissue.<sup>60</sup> Because esterases are key components of drug metabolism, these donors are highly versatile and can be altered to fit different scaffolding foundations among a variety of organ systems. The versatility of BW-HP-101 can be countered with further research into more specific enzyme-triggered donors.

Reactive oxygen species (ROS) are byproducts of electron transport chains located within mitochondria of biological cells; the production of these free radicals is vital to cell function because ROS signalling is imperative to inflammation regulation and cellular homeostasis while ROS can also display cytotoxic effects when being produced in excess.<sup>48</sup> Abundant ROS production has been correlated with several pathophysiological disease processes such as atherosclerosis and lipid peroxidation.<sup>47</sup> H<sub>2</sub>S displays cytoprotective properties when introduced to ROS like hydrogen peroxide and has

exhibited anti-apoptotic and antioxidant effects on cells. PeroxyTCM is a recently developed ROS-triggered  $H_2S$  donor that has utilized cytoprotective properties to counter the oxidative stress resulting from ROS.<sup>49</sup> However, introducing excess  $H_2S$  to cells is extremely toxic and can be detrimental to biological functioning.  $H_2S$ -ROS interactions and their role in regulating redox signalling is relatively new and must be further studied.

Thiol-triggered donors, including thiol-activated *gem*-dithiolbased  $H_2S$  donors (TAGDDs) and S-aroylthiooximes (SATO), are the most common type of  $H_2S$  donors due to the abundance of thiol molecules, such as cysteine, within biological organisms; the broad availability of thiol molecules makes it advantageous for donors to successfully release  $H_2S$  across the body.<sup>50, 51</sup> Some types of thiol-triggered donors are activated by the breaking of the S-S bond; this is a relatively simple mechanism that can have many applications upon further research. Polysulfide specifically is constructed from several S-S bonds and therefore has a large reservoir of potential for  $H_2S$  donor development. Glutathione, reduced glutathione, is a naturally occurring thiol that has been targeted for similar donor development to serve as a trigger due to its abundance and evidenced quick release of  $H_2S$ .<sup>50</sup>

## Different Strategies to Synthesize Hydrogen Sulfide-Releasing Biomaterials

Multiple studies have clearly indicated the pivotal roles of pretreatment of  $H_2S$  donors in different diseases.<sup>61-63</sup> However, many  $H_2S$  donors limit their direct applications due to poor water solubility, toxicity, low renal clearance rate and lacking regional specific release mechanism.<sup>21,64</sup> A variety of biological scaffolds developed in recent years are expected to become an effective means to solve the above constraints on the application of  $H_2S$ . Usually, the  $H_2S$  donor can be loaded on the biological scaffolds through physical incorporation or chemical conjugation. The resultant  $H_2S$ -releasing biomaterials could display a controllable, sustainable, and adjustable  $H_2S$  releasing.

## Doping biomaterials with H,S donors

The first strategy to synthesize H<sub>2</sub>S-releasing biomaterials is to fabricate biomaterials doping with H<sub>2</sub>S donors. This method has the advantages of easy operation, economy and convenient design. Specifically, the creation of biomaterial scaffolds incorporating with H<sub>2</sub>S donors can construct microenvironments for the release of H<sub>2</sub>S of donors under both in vitro and in vivo situations. In addition, these material scaffolds could provide various physical and chemical cues for specific cell signalling pathways, further expanding its application prospects in cardiovascular disease, wound healing, and regenerative medicine.<sup>52, 56, 65</sup> As shown in Figure 3A, fibrous scaffolds generated by electrospinning, which is a simple, cost-effective, and versatile technique, could be readily doped with H<sub>a</sub>S donors resulting in satisfied surface to volume ratio, variable porosity, and flexibility to form various sizes.66-68 Studies have reported an electrospinning of polycaprolactone (PCL), a structural polymer that can be modified into a threedimensional scaffolding matrix and chemically doped with H<sub>2</sub>S donors like NSHD1 and JK1 to create a fibrous material capable of releasing  $H_2S$  under specific pH conditions.<sup>52, 65</sup> These hybrids gave rise to prolonged  $H_2S$  releasing time compared to those donors alone.

Acidic linear polysaccharides such as alginate and hyaluronic acid (HA) are biocompatible macromolecules, which are able to form stable aqueous porous hydrogel by various strategies of crosslinking. As shown in Figure 3B, H<sub>2</sub>S-releasing sponge was fabricated by mixing the pH-dependent H<sub>2</sub>S donor JK-1 into an alginate sponge obtained by crosslinking sodium alginate with Ca<sup>2+</sup>. Those sponge-like materials stand out with their biocompatibility, biodegradability and ability to establish a three-dimensional-structural humid environment within wound regions.<sup>69-71</sup> This approach could be readily employed with different polysaccharide-based hydrogel systems.56, 57 Similar to those with H<sub>2</sub>S-releasing electrospinning fibres, H<sub>2</sub>S-releasing hydrogels/sponges could also significantly prolong H<sub>2</sub>S release half-lives, which will greatly expand the effective time window and application fields within different donor concentrations.

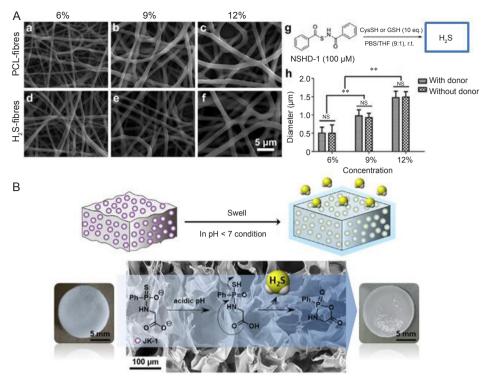
## Integrating H<sub>2</sub>S donors into biomaterials

Another strategy to synthesize the H<sub>2</sub>S-releasing biomaterials is to directly conjugate H<sub>2</sub>S-releasing functional units into different polymers and macromolecules like peptides. This will overcome the polydispersity caused by conventional doping methods. In a pioneer work by Matson and coworkers, a cysteine-triggered H<sub>2</sub>S donor SATO was conjugated into amphiphilic polymers to make micelles with a diameter of 20-100 nm (Figure 4A). Upon triggering with cysteine, a controlled release of H<sub>2</sub>S could be achieved with a prolonged release half-life, long bloodstream circulation and targeted regional specificity.72, 73 Using a similar strategy, the Matson group<sup>74</sup> developed a peptide-H<sub>2</sub>S donor conjugates supramolecular nanofibres loading with cysteine-triggered H<sub>2</sub>S donor SATO. These H<sub>2</sub>S releasing peptides will spontaneously result in discrete, stable supramolecular nanostructures with the capacity to delivery H<sub>2</sub>S (Figure 4B).<sup>74</sup> Conjugation of SATO into aromatic peptide amphiphiles hydrogel, enabling controllable H<sub>2</sub>S release and mechanical properties of hydrogel, results in a sustainable and controllable H<sub>2</sub>S release profile.<sup>75,76</sup> These H<sub>2</sub>S releasing biomaterials represent elegant examples to employ synthetic strategy to empower the biomaterials with an improved H<sub>2</sub>S release profile which can be used in a variety of biological applications taking advantage of the cardioprotective, anti-oxidative, and anti-inflammatory effects of H<sub>2</sub>S.

# Application of Hydrogen Sulfide-Releasing Biomaterials

# Cardiovascular disease

Cardiovascular disease was among the first explored areas of  $H_2S$  application due to its strong link with hypoxia, ROS production and cardioprotection. A significant decrease in the concentration of  $H_2S$  in blood plasma had been observed in patients with coronary heart disease.<sup>77</sup> Briefly, the pathways implicated in the cardioprotective effects of  $H_2S$  are multiple, involving  $K_{ATP}$  channels, regulation of mitochondrial respiration, and regulation of cytoprotective genes such as

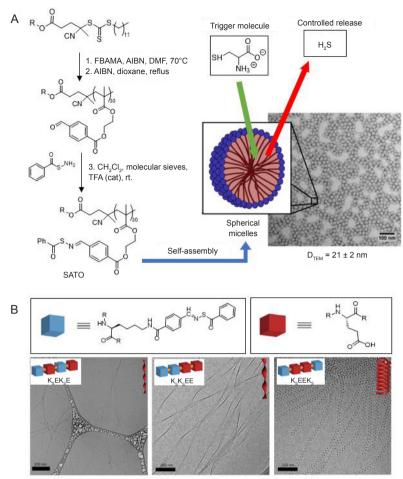


**Figure 3.** Physical incorporation of H<sub>2</sub>S donor into biomaterials. (A) H<sub>2</sub>S-release fibres by incorporating thiol-dependent H<sub>2</sub>S donor, NSHD-1, in the electrospun PCL-fibres: SEM images of H<sub>2</sub>S-fibres (a–c) and PCL-fibres (d–f). All images share the same scale bar (5 μm) in f. (g) The H<sub>2</sub>S donor, NSHD-1, can release H<sub>2</sub>S in the presence of cysteine or GSH. (h) Fibre diameters plot as a function of solution concentrations. The dopant, NSHD1, has no obvious effect on fibre diameters.<sup>65</sup> (B) H<sub>2</sub>S-releasing sponge sodium alginate/JK-1 by incorporating the pH-dependent H<sub>2</sub>S donor JK-1 into an alginate sponge obtained by crosslinking sodium alginate with Ca<sup>2+, 57</sup> Reprinted from Feng et al.<sup>65</sup> and Zhao et al.<sup>57</sup> Copyright 2015 and 2020, with permission from Elsevier Ltd. GSH: glutathione; NSHD-1: N-(benzoylthio) benzamide; PCL: polycaprolactone; SEM: scanning electron microscope.

nuclear factor erythroid 2-related factor-2 to further modulate the response under hypoxia condition, vasodilatation as well as cryoprotection and anti-inflammatory effects.78 Studies of effects of H<sub>a</sub>S on the cardiovascular system have been detailed and collected in previous literatures.<sup>42, 78, 79</sup> In a rat model of myocardial infarction, it was noted that a treatment of sodium hydrosulfide could significantly decrease the infarct size with a lower mortality risk.78,80 Exogenous H<sub>2</sub>S exhibits cardioprotection via the alleviation of left ventricular structural impairment in ischemia-induced heart failure.81 Based on understanding of roles of H<sub>2</sub>S in cardioprotection, treatment with inorganic donors like NaHS or other synthesized H<sub>2</sub>S-releasing donors, such as s-diclofenac, ADT-OH (5-(4-hydroxyphenyl)-3H-1,2-dithiole-3-thione), JKs and GYY4137, on both cardiomyocytes and animal models could help protect hearts from myocardial ischemia/reperfusion injuries by their intrinsic properties and/or incorporating with biomaterials (Figure 5).45, 81-85 In addition, considering its potential role in anti-inflammatory application,<sup>86-88</sup> H<sub>2</sub>S donors like NaHS could attenuate the development of atherosclerosis through a variety of mechanisms; notably the suppression of tumour necrosis factor-a-induced mRNA, expression of intercellular adhesion molecule 1 and vascular cell adhesion molecule 1, mRNA expression of P-selectin and E-selectin, and monocyte adhesion to human umbilical vein endothelial cells.<sup>89</sup>

Integrating H<sub>2</sub>S donors with biomaterials can facilitate in situ

delivery of H<sub>2</sub>S and provide both physical and chemical cues for other reactions. Under this strategy, Zhang et al.<sup>90</sup> selected large porous microspheres, a widely studied drug vehicle for pulmonary delivery, loaded with H<sub>2</sub>S donor ACS14 (S-aspirin) as an inhalational drug; an observable delay and even reversal in the progression of pulmonary arterial hypertension in a rat model resulted from this experimentation. Wang and Matson<sup>91</sup> utilized peptide-H<sub>2</sub>S donor conjugates supramolecular nanofibres saturated with cysteine-triggered H<sub>2</sub>S donor SATO to delay the occurrence of the peak time of H<sub>2</sub>S release, which was coupled with a prolonged release time as well as the mitigation of the doxorubicin-induced cardiotoxicity of the H9C2 cardiomyocyte. The integration of the SATO donor into aromatic peptide amphiphiles hydrogels was characterized by a secured H<sub>2</sub>S release and better mechanical properties. Cell viability and proliferation were subsequently increased and the migration of human umbilical endothelial cells was evidently more profound in studies on human tissue compared to the conventional H<sub>2</sub>S donor NaHS.<sup>75, 76</sup> Similar results have been shown in another study using ACS14 with chitosan/HA hydrogel.<sup>92</sup> Liang et al.<sup>93</sup> introduced a partially oxidized alginate grafting H<sub>2</sub>S donor 2-aminopyridine-5-thiocarboxamide (ALG-CHO-APTC) which exhibited excellent rheological and adhesion properties to adipose-derived stem cells. The injection of this multifunctional hydrogel into the Sprague-Dawley rat model had significantly upregulated cardiac-



**Figure 4.**  $H_2S$  donor units covalently linked to material backbones. (A)  $H_2S$ -releasing SATO-unit was incorporated to the polymer, which could be self-assembled into spherical micelles with an average diameter of  $21 \pm 2$  nm. Reprinted from Foster et al.<sup>72</sup> (B) Three isomeric peptide– $H_2S$  donor conjugates assembled into twisted ribbons and nanocoils in aqueous solution. Reprinted from Wang et al.<sup>74</sup> AIBN: 2,2'-azobis(2-methylpropionitrile; DMF: dimethylformamide; FBEMA: 2-(4-formylbenzoyloxy)ethyl methacrylate;  $H_2S$ : hydrogen sulfide; rt: room temperature; SATO: S-aroylthiooxime; SEM: scanning electron microscope; TFA: trifluoroacetic acid.

related mRNA and angiogenic factors while simultaneously downregulating inflammatory factors; furthermore, cardiac function was overall improved. Interestingly, Mauretti et al.<sup>94</sup> introduced a polyethylene glycol-fibrinogen hydrogel loading with serum albumin microbubbles coated with the H<sub>2</sub>S synthesis enzyme thiosulfate cyanide sulphurtransferase in a cardiac tissue repairment study. This novel three-dimensional scaffold improved cell growth of human cardiac progenitor cells and set the foundation for further assessment of the effects of H<sub>2</sub>S on cardiac muscle regeneration.

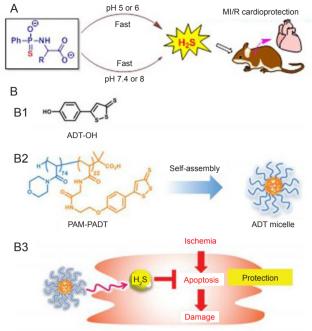
### Wound healing

The proliferation and differentiation of the epidermis are pivotal to wound healing and are often diminished under various pathological conditions such as diabetes mellitus, chronic skin wounds, and epidermal cancers.<sup>95-97</sup> The impairment of fibroblast proliferation and angiogenesis as well as a dysfunction of keratinocytes have been observed in diabetes mellitus patients and those suffering from chronic wounds;<sup>98-101</sup> however, exogenous and endogenous H<sub>2</sub>S could increase the proliferation and differentiation of the epidermis and promote angiogenesis in a dose-dependent manner.<sup>102-107</sup>

The inhibition of endogenous  $H_2S$  as experienced by a genetically modified CSE<sup>-/-</sup> mice model significantly decreased the rate of wound healing compared to the CSE<sup>+/+</sup> wild type mice.<sup>106, 108</sup> Meanwhile, lower level  $H_2S$  in plasma of diabetic patients, accompanied with vascular inflammation and overproduction of oxidants, could indicate the potential application of exogenous  $H_2S$  in diabetic wound healing.<sup>109, 110</sup> The role and corresponding mechanism of  $H_2S$  in wound healing are collected and detailed in previously published reviews.<sup>95, 106, 111</sup>

Although significant advances have been achieved, the applications of  $H_2S$  donors are still limited by the open-air and pH-variable wound environments. An ideal wound dressing should be biocompatible, antigen-free, elastic, and anti-inflammatory with the abilities to prevent infections, provide moisture, absorb fluids and exudates, and facilitate cell adhesion and growth factor release.<sup>112-114</sup> To satisfy these requirements, Wang and coworkers have utilized the electrospinning of PCL chemically doped with  $H_2S$  donors like NSHD1 (N-(benzoylthio) benzamide) and JK1 to create a  $H_2S$ -releasing fibrous material under specific pH conditions.<sup>52, 65</sup>

Review



Cardiomyocyte

**Figure 5.**  $H_2S$  donors act in cardiovascular disease. (A) JK1 gives rise to faster  $H_2S$  release under acidic condition, of which is distinctive feature of ischemia microenvironment compared to normal physiological condition. Reprinted with permission from Kang et al.<sup>45</sup> Copyright © 2016 American Chemical Society. (B)  $H_2S$  donor micelles protect cardiomyocytes from ischemic cell death. (B1) Chemical structure of ADT-OH. (B2) A block copolymer having ADT-groups (PAM-PADT) forms ADT micelles by self-assembly. (B3) Intracellular release of  $H_2S$  from ADT micelles prevents apoptotic damage of cardiomyocytes under ischemic condition. Reprinted with permission from Takatani-Nakase et al.<sup>45</sup> Copyright © Royal Society of Chemistry 2017. ADT: anethole dithiolethione; ADT-OH: 5-(4-hydroxyphenyl)-3H-1,2-dithiole-3-thione;  $H_2S$ : hydrogen sulfide; PAM-PADT: poly (N-acryloy morpholine)-poly anethole dithiolethione.

ROS-treated cells and the re-epithelialization through the upregulation of mRNA expression in genes such as collagen type I and collagen type III commonly expressed during wound healing processes.<sup>65</sup> Because H<sub>2</sub>S release has been shown to accelerate under an acidic pH, pH-sensitive H<sub>2</sub>S donors like JK1 can be incorporated to PCL scaffolding and subsequently promote the epithelial regeneration and healing when utilized for acute trauma wounds. The accelerated wound healing might be attributed to the increase of the wound closure rates, the augmentation of collagen density in the mice wound model, or the cell viabilities of fibroblasts *in vitro*.<sup>52</sup>

Hydrogels of linear polysaccharides such as alginate and HA are biocompatible, biodegradable stable porous biomaterials and exhibit great potential applications for wound healing.<sup>69-71</sup> An alginate hydrogel incorporated with a  $H_2S$  donor such as JK1<sup>57</sup> or dissolved  $H_2S^{115}$  contributes to the improvement of cell proliferation and migration in addition to angiogenesis with an accelerated wound healing process. Wu et al.<sup>56</sup> introduced a HA hydrogen incorporated with the JK1  $H_2S$  donor (**Figure 6**). Remarkably, compared to either component alone, this HA-JK1 hybrid hydrogel dressing yielded enhanced cell proliferation and angiogenesis as well as macrophage polarization towards M2 phenotype. This result has suggested a downregulation of the inflammation response which could be employed in the treatment of delayed diabetic wounds and other chronic wounds under various pathological conditions.

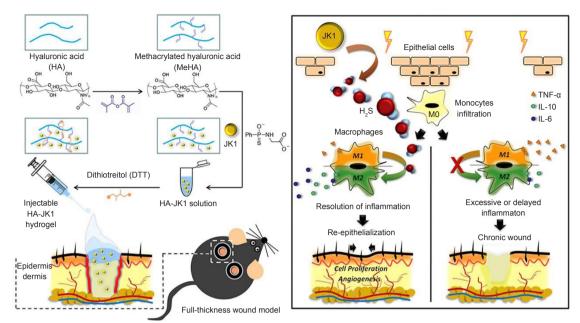
Lian et al.<sup>116</sup> utilized blended recombinant spider silk protein

to make a nanofibrous membrane incorporated with NaHS as a substrate to culture endothelial progenitor cells. This recombinant spider silk protein/NaHS/endothelial progenitor cell complex could significantly enhance wound regeneration efficiency and be utilized in skin tissue regeneration. To further expand upon  $H_2$ S-releasing biomaterial functionality, Liu et al.<sup>117</sup> proposed a multi-functional polymersome wound dressing spray, incorporating PCL with SATO and a positively charged peptide; together, the system gives rise to  $H_2$ S release and anti-bacterial properties at the same time and aids diabetic wound healing in improving angiogenesis, employing antibacterial properties and encouraging the proliferation of endothelial and epidermal cells.

#### Other clinical applications

H<sub>2</sub>S-releasing biomaterials can be employed in various physiological and pathophysiological situations outside direct application in cardiovascular disease or wound healing processes. In experiments with Staphylococcus aureus, which is commonly found at the wound site, fabricated SATO-aromatic peptide amphiphiles biofilm has shown significant antimicrobial effects.<sup>118</sup> This indicates that this biofilm hydrogel can be applied in situations where antimicrobial properties are critical for the treatment process. Injection into the intervertebral disc joint cavities in rat models experiencing intervertebral disc degeneration, a collagen-JK1 hydrogel expressed the ability to protect the disc from degeneration

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**Figure 6.** Schematic illustrating the preparation of injectable HA-JK1 hydrogel and its application to full-thickness dermal wound. (Left) JK1, as  $H_2S$  donor, was incorporated in the HA based injectable hydrogel, which can be used in the mouse wonder model system. (Right) The local low pH condition near the wound could promoted the fast release of  $H_2S$  of JK1, which could effectively accelerate the wound healing through promoting cell proliferation, angiogenesis and more importantly, suppressing inflammation via inducing M2 macrophage polarization. Reprinted from Wu et al.<sup>56</sup> Copyright 2019, with permission from Elsevier Ltd.  $H_2S$ : hydrogen sulfide; HA: hyaluronic acid; IL: interleukin; TNF- $\alpha$ : tumour necrosis factor- $\alpha$ .

via inhibiting the apoptosis of nucleus pulposus cells and in turn, alleviating the degradation of the disc's extracellular matrix.<sup>119</sup> In addition, when cultured with mesenchymal stem cells, Cacciotti et al.<sup>120</sup> have shown that when poly lactic acid nanofibres are doped with a H<sub>2</sub>S donor derived from garlic oil-soluble extract, a strong biocompatibility, antimicrobial activity, and protective properties against ROS were observed. Raggio et al.<sup>121</sup> introduced a silk fibroin scaffold loading with GYY4137, to bone tissue engineering with better displayed biocompatibility and no cytotoxicity. Apart from the treatment applications for these diseases we mentioned above, anti-cancer effect of H<sub>a</sub>S-releasing biomaterial has arisen attentions of many researchers because H<sub>2</sub>S as an antioxidant can suppress tumour growth by blocking proliferation of cancer cells, and by modulating differentiation of cancerassociated fibroblasts.<sup>122-124</sup> In Dao et al.'s work,<sup>125</sup> polyethylene glycol-cholesteryl conjugate polymer doping with trisulfide as H<sub>2</sub>S donor has shown attenuation of intracellular ROS and collagen type I production in breast cancer and potential in future clinical chemotherapy applications. Liu et al.<sup>126</sup> reported an anethole dithiolethione-loaded magnetic nanoliposome) delivery system, which can facilitate in situ drug delivery of H<sub>2</sub>S and magnetic resonance imaging of tumour at the same time. In summary, the recent advances of H<sub>2</sub>S-releasing biomaterials in applications as summarized in Table 1 will pave the ways to further mechanism studies and clinical applications.

# Conclusion

There was accumulating evidence from the last decade that demonstrated the potential of  $H_2S$ -releasing biomaterials for various biomedical applications. Further exploration of the molecular mechanisms underlying  $H_2S$  donors and their

function when incorporated with various biomaterials will potentially help us to understand the pathophysiological mechanisms of different diseases and assist the development of  $H_2S$ -based therapies. On the other hand, there is still a desperate need to develop novel  $H_2S$ -release donor molecules and biomaterials to address the demand for different therapies. In particular, recent progress in biomaterials science and technology will provide more opportunities to develop customized  $H_2S$ -releasing biomaterials with improved biocompatibility and optimized  $H_2S$  release profiles which can offer better answers to clinical challenges.

#### Author contributions

JF and QW conceived of the overall outline of the paper. JF, EP and QW contributed to the conception and design of all figures and the related literature survey. All authors contributed to the writing of the final manuscript.

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## Conflicts of interest statement

### No conflicts to disclose.

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#### Data sharing statement

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Application	H <sub>2</sub> S donor/ biomaterials	Research model	Effects/outcome	Proposed mechanism	Reference
Cardioprotection	NaHS	Murine infarction model	Infarcted size and mortality significantly decreased	Upregulation of Bcl-2, demoted expression of Bax, IL-1β and Caspase 3	80-82, 84
	JKs	H9C2 cardiomyoblasts & murine ischemia/ reperfusion model	A dose-dependent		45
		-	inhibition in cell viability; significantly reduced AAR/LV and INS/AAR		
	S-diclofenac	Rabbit model	Improved reperfusion pressure, anti-ischemic activity, activation of KATP channel		83
	DAT-MSN	Cardiomyocyte, murine infarction model	inhibited myocardial inflammation, greater reduction in the infarct	Same as above	84
			area and preserved cardiac ejection fraction		
	GYY4137	Cardiomyocyte, murine infarction	Infarcted size reduced, improved cardiac functions	Same as above	84
	ADT-OH/ PAM-PADT micelles	Rat cardiomyocytes	Rescue cells from apoptosis		85
	PHDCs/SATO	H9C2 cardiomyoblasts	Mitigated Dox-induced toxicity		91
	ALG-CHO/ APTC/ADSC	ADSC/rat model	Improved heart function	Suppressed TNF- <i>a</i> , upregulation of genes related to angiogenesis and cardiac function	93
	PFHy-MBs/ CST	hCPCs	Improved cell growth		94
Atherosclerosis	NaHS	Apolipoprotein-E K.O. mice model & HUVEC	Antiatherogenic effect with promoted cell viability	Inhibited ICAM-1 and TNF-α signalling	86, 89
	APA/SATO	HUVEC	Improved cell proliferation and migration		75,76
	Chitosan/ HA hydrogel/ ACS14	Platelet, rat model	Reduced inflammatory and AS lesion		92
Pulmonary arterial hypertension	LPM/ACS14	PAH rat model, HPAEC	Delayed and reversed progression of PAH	Suppressed NF-ĸB-Snail pathway	90
Wound healing	NaHS	HaCaT cell model, human epidermal melanocytes, HUVEC diabetic mice model	Promoted viability and differentiation	Promoted proliferation and differentiation via ATG5, TRP-1 signalling, angiogenesis via ANG-1, anti-inflammatory effect suppressing IL-6, TNF-α and MMP-9	102-105
	Na2S	HUVEC, diabetic mice model	Suppressed inflammation, promoted migration and proliferation	Upregulation of KATP/ P38/ERK/MAPK/VEGF signalling, and VEGFR2 transcription	106, 108
	NSHD1/PCL fibre	NIH 3T3, H9C2 cell model	Significantly prolonged release time, decreased ROS production		65
	JK1/PCL fibre	NIH 3T3, mice model	Enhanced wound regeneration, prolonged release time		52

**Table 1. Continued** 

	H <sub>2</sub> S donor/				
Application	biomaterials	Research model	Effects/outcome	Proposed mechanism	Reference
	JK1/HA hydrogel	Mice model	Fast wound healing with enhanced cell proliferation and angiogenesis	Macrophage polarization towards M2 phenotype, suppressed TNF-α	56
	JK1/SA hydrogel	L929 cell, rat model	Enhanced wound healing, promoted release profile		57
	H <sub>2</sub> S/SA hydrogel	L929 cell, rat model	Promoted wound healing in a dose dependent manner		115
	NaHS/rMaSp fibre	NIH 3T3, mice model	Promoted wound healing with EPC		116
	SATO/PCL fibre	NHEK cells, diabetic mice model	Bacterial inhibition, promoted diabetic wound healing		117
Anti-bacterial	SATO/APA biofilm/ dipeptides	Staphylococcus aureus	Inhibited bacterial growth		118
Intervertebral disc degeneration	JK1/Col hydrogel	Rat model, NP cell	Inhibited inflammatory process and cell apoptosis	Suppressing TNF- $\alpha$ , NF- $\kappa$ B, IL-1 $\beta$ expression and deactivation of P65 signalling	119
Tissue engineering	GaOS/PLA membrane	Cardiac mesenchymal stem cell	Promoted proliferation with reduced oxidative damage		120
	GYY4137/ fibroin scaffold	Mouse fibroblast, hBMSC	Enhanced cell viability		121
Anti-cancer	Trisulfide/ PEG- cholesteryl	MCF7 breast cancer cell	Suppressed tumourigenesis	Normalization of COL-1 expression	125
	ADT/AML	HepG2 cell, mice xenograft model	Reduction of tumour size, facilitate magnetic resonance imaging		126

Note: AAR: area-at-risk; ACS14: S-aspirin; ADSC: adipose-derived stem cell; ADT: anethole dithiolethione; ALG-CHO: partially oxidized alginate; AML: ADT-loaded magnetic nanoliposome; APA: aromatic peptide amphiphiles; APTC: 2-aminopyridine-5-thiocarboxamide; ATG5: autophagy related 5; COL-1: collagen type I; CST: cyanide sulphurtransferase; ADT-OH: 5-(4-hydroxyphenyl)-3H-1,2-dithiole-3-thione; EPC: endothelial precursor cell; ERK: extracellular signal-related kinase; GaOS: casting garlic oil-soluble extract; H2S: hydrogen sulfide; HA: hyaluronic acid; hBMSC: human bone marrow stromal cell; hCPC: human cardiac progenitor cell; HPAEC: human pulmonary artery endothelial cell; HUVEC: human umbilical vein endothelial cell; IL: interleukin; INS: infarct size; LV: lentivirus; MAPK: mitogen-activated protein kinase; MB: microbubble; MMP-9: matrix metallopeptidase 9; NF- $\kappa$ B: nuclear factor  $\kappa$ B; NSHD1: N-(benzoylthio)benzamides derivatives 1; PADT: poly anethole dithiolethione; PAH: poly (N-acryloy morpholine); PCL: polycaprolactone; PEG: polyethylene glycol; PFHy: polyethylene glycol-fibrinogen hydrogel; PHDC: peptide-H2S donor conjugate; PLA: poly lactic acid; rMaSp: recombinant spider silk protein; SA: sodium alginate; SATO: S-aroylthiooximes; TNF- $\alpha$ : tumour necrosis factor- $\alpha$ ; TRP-1: tyrosinase-related protein-1; VEGF: vascular endothelial growth factor; VEGFR2: vascular endothelial growth factor

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